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Acoustic Localisation of Coronary Artery Disease

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Contents						
Conte	nts					

- • Jump Viscoelasticity and wave equations
- • Acoustic Localisation of Coronary Artery Disease (CAD)
- • Jump High Order (in time) Space-Time FEM

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Viscoelasticity

PDE's with memory

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Mississippetints						

• Viscoelastic materials exhibit memory

Details

Application areas:

- damping (polymers)
- structures (concrete)
- porous media (geomechanics)
- electromagnetics (Debye media)
- on-Fickian diffusion
- soft tissue biomechanics

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Viscoelasticit	v				

- Viscoelastic materials exhibit memory
- which manifests as:
 - creep



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Viscoelasticit	v				

- Viscoelastic materials exhibit memory
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 - relaxation



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 - relaxation
 - hysteresis
 - frequency dependence



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Viscoelasticit	v					

- Viscoelastic materials exhibit memory
- which manifests as:
 - creep
 - relaxation
 - hysteresis
 - frequency dependence
- Typically described by partial differential equations with either
 - internal variables
 - or memory

Details

 $u_{tt} - \nabla^2 u = f - \nabla \cdot \sigma$ $\sigma_t + \gamma \sigma = \mu \nabla u$ $u_{tt} - \nabla^2 u = f - \int_0^t b(t-s) \nabla^2 u(s) \, ds$ Prony: $b(t) = \sum_{i} b_i e^{-t/\tau_i}$ or weakly singular: t^p or fractional calculus nonlinearity, e.g. $\gamma \leftarrow \gamma(u)$

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Details

 u_{t}

$$\begin{split} u_{tt} - \nabla^2 u &= f - \nabla \cdot \sigma \\ \sigma_t + \gamma \sigma &= \mu \nabla u \\ t - \nabla^2 u &= f - \int_0^t b(t-s) \nabla^2 u(s) \, ds \\ \text{Prony:} \qquad b(t) &= \sum_i b_i e^{-t/\tau_i} \\ \text{or weakly singular: } t^p \\ \text{or fractional calculus} \\ \text{nonlinearity, e.g. } \gamma \leftarrow \gamma(u) \end{split}$$

Analysis can exploit the fading memory: an example...

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Electromagnetism

Maxwell's equations — dispersive dielectrics

$$\nabla \times \mathbf{E} + \dot{\mathbf{B}} = 0 \qquad \nabla \cdot \mathbf{B} = 0$$
$$\nabla \times \mathbf{H} - \dot{\mathbf{D}} = \mathbf{J} \qquad \nabla \cdot \mathbf{D} = \mathbf{0}$$

What has this got to do with viscoelasticity? Dispersion...

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Electromagnetism

Maxwell's equations — dispersive dielectrics

$$\nabla \times \mathbf{E} + \dot{\mathbf{B}} = 0 \qquad \nabla \cdot \mathbf{B} = 0$$
$$\nabla \times \mathbf{H} - \dot{\mathbf{D}} = \mathbf{J} \qquad \nabla \cdot \mathbf{D} = \rho$$

What has this got to do with viscoelasticity? Dispersion...

 $B = \mu H$ but dielectric polarization is not instantaneous...

Debye: $\boldsymbol{D} = \varepsilon_0 (1 + \chi) \boldsymbol{E} + \boldsymbol{P}$ with $\tau \dot{\boldsymbol{P}} + \boldsymbol{P} = (\varepsilon_s - \varepsilon_\infty) \varepsilon_0 \boldsymbol{E}$

with P(0) = 0 and the ε 's known. Hence, we can use either of...

$$(arepsilon_0arepsilon_\infty)^{-1}oldsymbol{D}=oldsymbol{E}+\dot\psi*oldsymbol{E}\qquad ext{ or }\qquad arepsilon_0arepsilon_\inftyoldsymbol{E}=oldsymbol{D}+\dotarphi*oldsymbol{D}$$

which is viscoelasticity! Exploit related results...

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Electromagne	etism					

Example of a priori control. No Gronwall!

Find
$$\boldsymbol{D}$$
 such that: $\ddot{\boldsymbol{D}} + \nabla \times \mu^{-1} \nabla \times \boldsymbol{E} + \sigma \dot{\boldsymbol{E}} = -\dot{\boldsymbol{J}}_a,$
where $\varepsilon \dot{\boldsymbol{E}}(t) = \dot{\boldsymbol{D}}(t) + \varphi'(t) \boldsymbol{D}(0) - \int_0^t \varphi_s(t-s) \dot{\boldsymbol{D}}(s) \, ds.$

Theorem

With
$$G(t) = -\dot{J}_a(t) - \sigma \varepsilon^{-1} \varphi'(t) D(0)$$
 known and if $\sigma > 0$ we have,

$$\begin{split} \mu \varepsilon \| \dot{\boldsymbol{D}}(t) \|_{0}^{2} + \check{\varphi} \| \nabla \times \boldsymbol{D}(t) \|_{0}^{2} + \mu \sigma \check{\varphi} \| \dot{\boldsymbol{D}} \|_{L_{2}(0,t;\boldsymbol{L}_{2}(\Omega))}^{2} \\ \leqslant \mu \varepsilon \| \dot{\boldsymbol{D}}(0) \|_{0}^{2} + \| \nabla \times \boldsymbol{D}(0) \|_{0}^{2} + \frac{\mu \varepsilon^{2}}{\sigma \check{\varphi}} \| \boldsymbol{G} \|_{L_{2}(0,t;\boldsymbol{L}_{2}(\Omega))}^{2}. \end{split}$$

Remark: similar results are possible if $\sigma = 0$.

Using also Rivera & Menzala's lemma (Quart. Appl. Math., LVII, 1999)

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Electromagnetism

Example: a discrete abstract wave equation

Relaxation (fading memory) expressed through internal variable rate equations: find $u: I \to V$ such that,

$$(\varrho \ddot{\boldsymbol{u}}(t), \boldsymbol{v}) + a(\boldsymbol{u}(t), \boldsymbol{v}) + b(\dot{\boldsymbol{u}}(t), \boldsymbol{v}) = \langle L(t), \boldsymbol{v} \rangle + \sum_{q=1}^{N_{\varphi}} a(\boldsymbol{u}_{q}^{\star}(t), \boldsymbol{v}) \ \forall \boldsymbol{v} \in V,$$

$$a(\tau_q \dot{\boldsymbol{u}}_q^{\star}(t) + \boldsymbol{u}_q^{\star}(t), \boldsymbol{v}) = a(\varphi_q \boldsymbol{u}(t), \boldsymbol{v}) \text{ for } q = 1, \dots, N_{\varphi}, \ \forall \boldsymbol{v} \in V.$$

And its DG-in-time approximation: find $(U,W)\approx (u,\dot{u})$ such that

$$\left(\!\!\left(\varrho\dot{W},\vartheta\right)\!\!\right)_n + \left(\varrho\left[\!\left[W\right]\!\right]_{n-1},\vartheta_{n-1}^+\right) + a\left(\!\left[U,\vartheta\right]\!\right)_n + b\left(\!\left(W,\vartheta\right)\!\!\right)_n - \sum_{q=1}^{N\varphi} a\left(\!\left[Z_q,\vartheta\right]\!\right)_n = \left<\!\!\left[L,\vartheta\right]\!\!\right]_n$$

$$a\left(\!\left(\dot{U}-W,\zeta\right)\!\!\right)_n + a\left(\!\left[U\right]\!\!\right]_{n-1},\zeta_{n-1}^+\right) = 0,$$
for $q = 1, \dots, N_{\varphi}$

$$a\left(\!\left(\tau_q\dot{Z}_q + Z_q - \varphi_q U, \xi_q\right)\!\!\right)_n + a(\tau_q\left[\!\left[Z_q\right]\!\right]_{n-1},\xi_{q,n-1}^+) = 0,$$

for all test functions θ , ζ , $\xi_1, \ldots \in \mathbb{P}_r(I_n; V^h)$.

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Sharp discrete stability

The discrete scheme...

$$\begin{split} \left(\!\!\left(\varrho\dot{W},\vartheta\right)\!\!\right)_n + \left(\varrho\left[\!\!\left[W\right]\!\!\right]_{n-1},\vartheta_{n-1}^+\right) + a\left(\!\!\left(U,\vartheta\right)\!\!\right)_n + b\left(\!\!\left(W,\vartheta\right)\!\!\right)_n - \sum_{q=1}^{N_{\varphi}} a\left(\!\!\left(Z_q,\vartheta\right)\!\!\right)_n = \left<\!\!\left(L,\vartheta\right)\!\!\right)_n \\ & a\left(\!\!\left(\dot{U}-W,\zeta\right)\!\!\right)_n + a\left(\!\!\left[U\right]\!\!\right]_{n-1},\zeta_{n-1}^+\right) = 0, \\ \text{for } q = 1, \dots, N_{\varphi} \qquad a\left(\!\!\left(\tau_q\dot{Z}_q + Z_q - \varphi_q U,\xi_q\right)\!\!\right)_n + a(\tau_q\left[\!\left[Z_q\right]\!\!\right]_{n-1},\xi_{q,n-1}^+\right) = 0, \\ \text{satisfies, for each time } t_m, \\ e^{1/2}W_m^- \|_0^2 + \|\varphi_0^{1/2}U_m^-\|_V^2 + \sum_{m=1}^{N_{\varphi}} \left\| \frac{Z_{q,m}^- - \varphi_q U_m^-}{2} \right\|_{+2}^2 \int_{-2}^{t_m} \left(\!\!\left(\sum_{m=1}^{N_{\varphi}} \left\| \frac{Z_q - \varphi_q U}{2} \right\|_{+2}^2 + b(W,W)\right) \right) dt \\ \end{split}$$

$$\begin{split} e^{2/2} W_m \|_0^2 + \|\varphi_0^{-\gamma} - U_m\|_V^2 + \sum_{q=1}^{2} \left\| \frac{1}{\sqrt{\varphi_q}} \right\|_V^2 + 2\int_0^2 \left(\sum_{q=1}^{2} \left\| \frac{1}{\sqrt{\tau_q \varphi_q}} \right\|_V + b(W, W) \right) dt \\ + \sum_{n=1}^m \left(\sum_{q=1}^{N_\varphi} \left\| \left\| \left[\frac{Z_q - \varphi_q U}{\sqrt{\varphi_q}} \right] \right\|_{n-1} \right\|_V^2 + \|\varrho^{1/2} \left[W \right]_{n-1} \|_0^2 + \|\varphi_0^{1/2} \left[U \right]_{n-1} \|_V^2 \right) \\ &= 2\int_0^{t_m} \langle L, W \rangle \, dt + \|\varrho^{1/2} W_0^- \|_0^2 + \|\varphi_0^{1/2} U_0^- \|_V^2. \end{split}$$

Leads to Non-Gronwall discrete stability. (Error bounds?)

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Coronary Artery Disease

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Coronary Artery Disease (CAD)

Coronary Artery Disease (CAD)



- In the UK in 2010 CAD caused over 14% of all deaths (80,568/561,666).
 - About 95% in people aged 55+ yrs.
- €7.5 billion approx 2009 cost...
 - €2 billion healthcare (*per capita* €32)
 - €3.5 billion lost productivity
 - €2 billion informal patient care
- An expensive killer huge tax burden.
- Poor diet & ageing population will exacerbate problem.

Source: Tables 6.2, 6.3, Coronary Heart Disease Statistics. A compendium of health statistics. 2012 ed. British Heart Foundation. ISBN 978-1-899088-12-6

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What is Coronary Artery Disease?

- Lipids & calcium deposits form atheromatous plaques between endothelium and artery wall
- Stenosis grows and reduces artery calibre.
- Vulnerable plaque suddenly ruptures causes clot
- Myocardial Ischaemia/Infarction: a 'heart attack'

What can mathematics offer?

- biotissue highly viscoelastic and hysteretic
- acoustic shear waves caused by stenotic wake disturbance travel at frequency-dependent speed
- 150–750 Hz signals detectable at chest surface
- Exploit this for non-invasive computational diagnosis of arterial stenosis via inverse problem
- Challenging and ambitious: at a very early stage...

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Localised disturbance: illustrative experiment...

Blood mimicking fluid pumped through artificially stenosed tube constrained within a TMM block (blue, forward; red, reversed).



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Coronary Artery Disease (CAD)

Semmlow and Rahalkar, Ann. Rev. Biomed. Eng. 2007 9:449-69

Acoustic Detection of Coronary Artery Disease

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Key Words

phonocardiography, heart sounds, coronary stenosis, coronary bruits, signal processing, cardiac microphones

Abstract

Coronary artery disease (CAD) occurs when the arteries to the heart (the coronary arteries) become blocked by deposition of plaque, depriving the heart of oxygen-bearing blood. This disease is arguably the most important fatal disease in industrialized countries, causing one-third to one-half of all deaths in persons between the ages of 35 and 64 in the United States. Despite the fact that early detection of CAD allows for successful and cost-effective treatment of the disease,

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Coronary Artery Disease

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Coronary Artery Disease (CAD)

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Key Finding... no other approach ... promises to be as inexpensive, simple...and risk free

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Coronary Artery Disease (CAD)

What can computational mathematics offer?

Scoping/Feasibility Project: Methods and Aims

- Use the signature chest surface signal for screening and diagnosis. (Expected range $\sim 150 \,\mathrm{Hz} 750 \,\mathrm{Hz}$.)
- In vitro biomechanics:
 - Characterize tissue mimicking agarose gel.
 - Build gel chest phantoms with controllable 'stenoses'.
 - Use a fluid loaded model to create shear waves.
- Computational Mathematics:
 - Material characterization through inverse problem data-fitting.
 - Simulations of wave transit through mimicked chest.
 - Stenosis localization through inverse solver.

EVENTUAL AIM noninvasive screening & diagnosis

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Acoustic Localisation of CAD

EPSRC

Engineering and Physical Sciences Research Council

Acoustic Localisation of Coronary Artery Stenosis

Brunel: EP/H011072/1 Queen Mary: EP/H011285/1 April 2010 — March 2014

Speculative Research

Multidisciplinary/international:

- Blizard (Queen Mary): chest phantom construction and experiments
- CRSC (North Carolina State): identification and inverse problem
- BICOM (Brunel): FE models & computation of direct problem

People: C Kruse, JR Whiteman, SE Greenwald, MJ Birch, MP Brewin, J Reeves, HT Banks, ZR Kenz, S Hu, B Kehra, E Cantor, D Mehta, I Gnaneswaren, S Shaw

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Acoustic Localisation of CAD

Schematics - first steps

The reality...



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sensors and signals

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Schematics - first steps

The reality...





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Schematics - first steps

The reality...



Proof of Concept: Agar Gel Chest Phantom



2D is computationally tractable at this early stage

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Length scales of interest

Vertical chest cross section.

10cm (approx)





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Figure 4b from Baumüller S, Leschka S, Desbiolles L, et al. Dual-source versus 64-section CT coronary angiography at lower heart rates: comparison of accuracy and radiation dose. Radiology 2009;253:56-64. (c) RSNA 2009

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Vertical chest cross section.

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The initial 2D rig – small scale at first



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The mathematical model — classical linear viscodynamics

 $\varrho \dot{\boldsymbol{w}} - \nabla \cdot \boldsymbol{\sigma} = \varrho \boldsymbol{f} + \text{initial and boundary data,}$

with $m{w}=\dot{m{u}}$ and constitutive relationship,

$$\underline{\boldsymbol{\sigma}}(t) = \underbrace{\underline{\boldsymbol{C}}\underline{\boldsymbol{\varepsilon}}(\boldsymbol{w}(t))}_{\text{Voigt}} + \underbrace{\underline{\boldsymbol{D}}\underline{\boldsymbol{\varepsilon}}(\boldsymbol{u}(t))}_{\text{Hooke}} + \underbrace{\underline{\boldsymbol{D}}}_{0} \underbrace{\int_{0}^{t} \varphi'(t-s)\underline{\boldsymbol{\varepsilon}}(\boldsymbol{u}(s))}_{\text{Maxwell/Zener}} ds$$

or internal variables for the Maxwell/Zener term,

$$\boldsymbol{z}_q(t) := \int_0^t \frac{\varphi_q}{\tau_q} e^{-(t-s)/\tau_q} \boldsymbol{u}(s) \, ds$$

Linearity!!!! Why? Justifiable? If not then is there any chance? ...

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Using the gel cylinder pictured earlier and the three outputs...



• We allow additive/multiplicative Gaussian noise on the signals.

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Current Status

Current progress on the localisation problem

Use: gel cylinder, embedded vibrator and three surface outputs...

Algorithm

- A ramped-up sinusoidal $500 \,\mathrm{Hz}$ axial-displacement source is placed at a known position \bar{z} in the central bore.
- The forward solver computes the axial displacement surface signal at heights 13 mm, 26 mm and 39 mm.
- These 'truth' data are 'banked' and may or may not be deliberately corrupted with additive noise: noisy truth = truth + $N_L \times \epsilon$ for N_L a noise level amplitude and $\epsilon \sim N(0, 1)$. (Or with multiplicative noise.)
- The position of the source \bar{z} is now 'forgotten'.
- matlab's fminsearch iteratively estimates \bar{z} given only the (noisy) truth and the forward solve outputs

Forward solver: Bicubic Galerkin finite elements were used on a 25×51 element mesh and with 24,000 Crank-Nicolson time steps for $0 \le t \le 1$ s.

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Some results for a $500 \,\mathrm{Hz}$ source signal.

Assume perfect knowledge of material constants. Examples of a 'true' signal and a corrupted version: additive Gaussian noise, amplitude 10^{-6} .



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Example: $500 \,\mathrm{Hz}$ with 10^{-6} noise



Well posed-ness seems to follow from a good starting value. Some robustness in the presence of significant measurement noise.

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Summary: 500 Hz with 10^{-6} noise



Well posed-ness seems to follow from a good starting value. Some robustness in the presence of significant measurement noise.

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Comparison: 500 Hz no noise (left) 10^{-6} noise (right)



Square indicate success: darker shades mean fewer iterations. Crosses represent failure.

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Comparison: 500 Hzhi-fi and noiseless (left), lo-fi with 10^{-6} noise (right)



Left: 25×51 mesh of bicubics, 24000 time steps Right: 25×51 mesh of bilinears, 12000 time steps

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- Little change of performance with lo-fi forward solves and very significant additive and multiplicative Gaussian signal-noise.
- Reasonably good initial guesses lead to correct localisation: end effects seem a problem.
- Each localization problem needs about 12 hours: need parallelism, further optimized code, ...
- Next step is to build and simulate a 3D virtual chest with phantom ribs, lungs, heart, arteries, skin and fat.

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High Order DG-in-time FEM

High Order Space-Time FEM for Wave Equations

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Space-Time Finite Elements

High order numerical schemes are known for...

- smaller dispersion error in wave propagation problems
- better work/accuracy ratios

We've developed temporally high order time-diagonalised space-time finite element codes for elasto- and visco-dynamics.

We use continuous spectral (i.e. Galerkin with Gauss-Lobatto) FEM in space and discontinuous Galerkin in time. • Jump

We can compute easily using fifth-degree space-time polynomial approximations.

Hi-Fi solutions are not necessarily important for inverse solvers but speed/parallelism is...

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Maut Chang						

Discretize a wave equation in time with DGFEM: for each n = 1, 2, ..., N in turn, find $(U, W)|_{I_n} \in \mathbb{P}_r(I_n; V) \times \mathbb{P}_r(I_n; V)$ such that

$$\begin{split} \int_{I_n} (\dot{W}(t), \vartheta(t)) &+ a(U(t), \vartheta(t)) \, dt + (\llbracket W \rrbracket_{n-1}, \vartheta_{n-1}^+) + a(\llbracket U \rrbracket_{n-1}, \zeta_{n-1}^+) \\ &+ \int_{I_n} a(\dot{U}(t), \zeta(t)) - a(W(t), \zeta(t)) \, dt = \int_{I_n} \langle L(t), \vartheta(t) \rangle \, dt \\ &\quad \forall \vartheta \in \mathbb{P}_r(I_n; V) \quad \text{and} \quad \forall \zeta \in \mathbb{P}_r(I_n; V), \end{split}$$

with IC's: $U_0^- := \breve{u}$ and $W_0^- := \breve{w}$; and $\mathbb{P}_r(I_n; X)$ the space of polynomials of degree r on the time interval I_n with coefficients in the target space X. Note that r could be n-dependent.

Diagonalize following: Werder, Gerdes, Schötzau and Schwab, CMAME 2001; 190:6685—6708.

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... then gives the decoupled form,

 $2\lambda_i(Y_i,\vartheta) + k_n a(Z_i,\vartheta) = 2F_i(\vartheta),$ $a(2\lambda_i Z_i - k_n Y_i,\vartheta) = 2\beta_i a(U_{n-1}^-,\vartheta)$

for $i = 0, 1, 2, \dots, r =$ the temporal polynomial degree.

This complex symmetric system requires just one matrix solve for each pair (Y_i, Z_i) and (U, W) are recovered from them.

In IJNME 2014, 98:131156 (DOI: 10.1002/nme.4631), we showed that expected convergence rates are obtained for temporal polynomial degrees up to seven.

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Next Steps

Spectral FE for CG-in-time heat equation



Using Gauss-Lobatto for time integration...

In SISC, 36:B1B13 (DOI: 10.1137/130914589), we showed that expected convergence rates are obtained for temporal polynomial degrees up to six.

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This is to some extent empirical. Unclear how it deals with

- variable coefficients
- nonlinearities
- dispersion error
- singularities

But it is suited to the coming many-core era...

And one can imagine several variant schemes.

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shameless advertising

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A last thought









$$\nabla^{2}\phi = 0 \qquad P^{2}\langle F, v \rangle_{H} = \langle f, v \rangle_{H} \quad \forall v \in H \quad x \leftarrow x^{2} + c \quad \nabla \times E + \dot{B} = 0$$

$$u_{t} + u \cdot \nabla u = \frac{1}{\rho} \nabla p + \mu \nabla^{2} u \quad \frac{\partial C}{\partial t} + \frac{\sigma^{2}S^{2}}{2} \frac{\partial^{2}C}{\partial S^{2}} + rS \frac{\partial C}{\partial S} = rC \quad \ddot{u} = c^{2} \nabla^{2} u$$

$$V_{t} = e^{-r(T-t)} \mathbb{E}_{Q}(X|S_{t}) \quad x_{n+1} = x_{n} - \frac{f(x_{n})}{f'(x_{n})} \quad -\sigma_{ij,j} = f_{i} \quad (uv)' = uv' + u'v$$

$$\vec{e}(u) := \frac{1}{2} \left(\frac{\partial u_{i}}{\partial x_{j}} + \frac{\partial u_{j}}{\partial u_{i}} \right) \quad Av = \lambda v \quad i\hbar \frac{\partial \psi}{\partial t} = -\frac{\hbar}{2m} \nabla^{2} \psi + V\psi$$

$$u(u, v) = f(v) \quad \forall v \in \dot{H}^{1}(\Omega) \quad \phi(y) = \psi(y) + \int_{\Omega} r(y - x)x(x)\phi(x) dx$$

$$\frac{dy}{dx} = \frac{dy}{du} \frac{du}{dx} \frac{dv}{dx} - \frac{1}{\sqrt{2\pi\sigma^{2}}} \exp\left(-\frac{(x - \mu)^{2}}{2\sigma^{2}} \right) \quad \frac{\partial u}{\partial k} - \nabla^{2} u = 0$$

$$\nabla \times H - \dot{D} = J \quad \frac{dS}{S} = \mu dk + \sigma dX \quad f(z_{0}) = \frac{1}{2\pi i} \int_{T} \frac{f(z)}{x - z_{0}} dz$$
Barts Health
NHS Trust
$$UG = \left(a \frac{\partial c}{\partial t} \frac{\cos c}{\cos c} - c + \frac{2 \cos c}{\cos t} + c + \frac{\cos u}{\cos t} \right) \quad (uv) = uv + u'v + u'$$

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A last thought









 $\nabla^2 \phi = 0 \quad _{B^{2}} \langle F, v \rangle_{B} = (f, v)_{B} \quad \forall v \in H \quad z \leftarrow z^2 + c \quad \nabla \times E + \dot{B} = 0$

The difference between theory and practice in practice is greater than the difference between theory and practice in theory Yogi Berra, Albert Einstein, ...



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A last thought









 $\nabla^2 \phi = 0 \quad {}_{B'} \langle F, v \rangle_B = (f, v)_B \quad \forall v \in H \quad z \leftarrow z^2 + c \quad \nabla \times E + \dot{B} = 0$

The difference between theory and practice in practice is greater than the difference between theory and practice in theory Yogi Berra, Albert Einstein, ...

THANK YOU FOR LISTENING



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Appendix — time permitting

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Time Diagonalisation

Consider a generic wave equation in weak form: find $u\colon L_2(0,T)\to V$ such that

$$\int_{I_n} (\dot{w}(t), v(t)) + a(u(t), v(t)) dt = \int_{I_n} \langle L(t), v(t) \rangle dt \quad \forall v \in L_2(0, T; V).$$

where: $I_n = (t_{n-1}, t_n)$, $w = \dot{u}$, V is a Hilbert space, $a: V \times V \to \mathbb{R}$ a symmetric bilinear form and $L: L_2(0,T) \to V'$ a time dependent linear form containing body loads and boundary tractions.

Discretize in time using Discontinuous Galerkin finite elements...

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Discretize in time with DGFEM: for each n = 1, 2, ..., N in turn, find $(U, W)|_{I_n} \in \mathbb{P}_r(I_n; V) \times \mathbb{P}_r(I_n; V)$ such that

$$\begin{split} &\int_{I_n} (\dot{W}(t), \vartheta(t)) + a(U(t), \vartheta(t)) \, dt + (\llbracket W \rrbracket_{n-1}, \vartheta_{n-1}^+) + a(\llbracket U \rrbracket_{n-1}, \zeta_{n-1}^+) \\ &+ \int_{I_n} a(\dot{U}(t), \zeta(t)) - a(W(t), \zeta(t)) \, dt = \int_{I_n} \langle L(t), \vartheta(t) \rangle \, dt \\ &\quad \forall \vartheta \in \mathbb{P}_r(I_n; V) \quad \text{and} \quad \forall \zeta \in \mathbb{P}_r(I_n; V), \end{split}$$

with the understanding that the initial conditions are $U_0^- := \breve{u}$ and $W_0^- := \breve{w}$. Here, for each n, we use $\mathbb{P}_r(I_n; X)$ to denote the space of polynomials of degree r on the time interval I_n with coefficients in the target space X. Note that r could be n-dependent.

Diagonalize following: Werder, Gerdes, Schötzau and Schwab, CMAME 2001; 190:6685—6708.

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$$\begin{split} \int_{I_n} (\dot{W}(t), \vartheta(t)) + a(U(t), \vartheta(t)) \, dt + (\llbracket W \rrbracket_{n-1}, \vartheta_{n-1}^+) + a(\llbracket U \rrbracket_{n-1}, \zeta_{n-1}^+) \\ + \int_{I_n} a(\dot{U}(t), \zeta(t)) - a(W(t), \zeta(t)) \, dt = \int_{I_n} \langle L(t), \vartheta(t) \rangle \, dt \\ \forall \vartheta \in \mathbb{P}_r(I_n; V) \quad \text{and} \quad \forall \zeta \in \mathbb{P}_r(I_n; V), \end{split}$$

Let $\{\phi_i : i = 0, 1, ..., r\}$ be a basis for $\mathbb{P}_r(I_n)$ and introduce the ansatz forms of the approximations to u and w on I_n as,

$$U(t)|_{I_n} = \sum_{j=0}^r \phi_j(t)U_j$$
 and $W(t)|_{I_n} = \sum_{j=0}^r \phi_j(t)W_j$

where $\{U_0, U_1, \ldots\}, \{W_0, W_1, \ldots\} \subseteq V$. Replacing each of $\vartheta(t)$ and $\zeta(t)$ with $\phi_i(t)\vartheta$ for $\phi_i \in \mathbb{P}_r(I_n)$ and $\vartheta \in V$ we obtain...

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~

$$\sum_{j=0}^{r} \int_{I_n} \dot{\phi}_j(t)\phi_i(t)(W_j,\vartheta) + \phi_j(t)\phi_i(t)a(U_j,\vartheta) dt$$
$$+ \sum_{j=0}^{r} \phi_{j,n-1}^+\phi_{i,n-1}^+(W_j,\vartheta) = \int_{I_n} \phi_i(t)\langle L(t),\vartheta\rangle dt + \phi_{i,n-1}^+(W_{n-1}^-,\vartheta)$$

and,

$$\sum_{j=0}^{r} \int_{I_n} \dot{\phi}_j(t)\phi_i(t)a(U_j,\vartheta) - \phi_j(t)\phi_i(t)a(W_j,\vartheta) dt$$
$$+ \sum_{j=0}^{r} \phi_{j,n-1}^+\phi_{i,n-1}^+a(U_j,\vartheta) = \phi_{i,n-1}^+a(U_{n-1}^-,\vartheta)$$

where each holds for all $\vartheta \in V$ and for each $i \in \{0, 1, \dots, r\}$.

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Define matrices via,

$$\mathsf{A}_{ij} := \int_{I_n} \dot{\phi}_j(t) \phi_i(t) \, dt + \phi_{j,n-1}^+ \phi_{i,n-1}^+ \text{ and } \mathsf{M}_{ij} := \int_{I_n} \phi_j(t) \phi_i(t) \, dt,$$

where *i* indexes the rows. Choosing basis functions as the image under the linear map from [-1, 1] to I_n of the normalized Legendre polynomials gives $2M = k_n I - diagonal!$

A is diagonalizable over \mathbb{C} for all polynomial degrees of practical interest ($r \leq 100$). Ref: Werder *et al.* CMAME 2001; 190:6685—6708.

In fact: $D = Q^{-1}AQ = \lceil \lambda_0 \cdots \lambda_r \rfloor$ where $\lceil \cdots \rfloor$ indicates a diagonal matrix of pairwise complex conjugate eigenvalues and where Q has complex entries.

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BIRS 16w5071: Comp & Num Anal Transient Problems in Acoustics, Elasticity, and Electromagnetism, Jan 17-22, 2016

Using the summation convention our system is:

$$\begin{split} \mathsf{A}_{ij}(W_j,\vartheta) + \delta_{ij}\frac{k_n}{2}a(U_j,\vartheta) &= \mathsf{F}_i(\vartheta), \\ \mathsf{A}_{ij}a(U_j,\vartheta) - \delta_{ij}\frac{k_n}{2}a(W_j,\vartheta) &= \mathsf{G}_i(\vartheta), \end{split}$$

where F_i and G_i contain known data.

Let $\{Y_q\}$ and $\{Z_q\}$ uniquely solve $W_j = Q_{jq}Y_q$ and $U_j = Q_{jq}Z_q$: $A_{ij}Q_{jq}(Y_q, \vartheta) + \delta_{ij}\frac{k_n}{2}Q_{jq}a(Z_q, \vartheta) = F_i(\vartheta),$ $A_{ij}Q_{jq}a(Z_q, \vartheta) - \delta_{ij}\frac{k_n}{2}Q_{jq}a(Y_q, \vartheta) = G_i(\vartheta),$

Premultiply with $R = Q^{-1}$, noting that,

$$\mathsf{R}_{pi}\mathsf{A}_{ij}\mathsf{Q}_{jq} = \delta_{pq}\lambda_p$$
 and $\mathsf{R}_{pi}\delta_{ij}\mathsf{Q}_{jq} = \delta_{pq}$,

and setting $F_i(\vartheta) := \mathsf{R}_{ip}\mathsf{F}_p(\vartheta)$ and $G_i(\vartheta) := \mathsf{R}_{ip}\mathsf{G}_p(\vartheta) \dots$

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... then gives the decoupled form,

 $2\lambda_i(Y_i,\vartheta) + k_n a(Z_i,\vartheta) = 2F_i(\vartheta),$ $2\lambda_i a(Z_i,\vartheta) - k_n a(Y_i,\vartheta) = 2G_i(\vartheta)$

for $i = 0, 1, 2, \dots, r =$ the temporal polynomial degree.

This complex symmetric system requires just one matrix solve.

In IJNME 2014, 98:131156 (DOI: 10.1002/nme.4631), we showed that expected convergence rates are obtained for temporal polynomial degrees up to seven.

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Spectral FE for CG-in-time heat equation



Using Gauss-Lobatto for time integration...

In SISC, 36:B1B13 (DOI: 10.1137/130914589), we showed that expected convergence rates are obtained for temporal polynomial degrees up to six.

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